

Automatic Analysis of the Electrocardiogram

Electrocardiography has recently seen ~~many~~ several
several the technical improvements

Electrocardiography has ~~long been~~ ^{become} one of the
most valuable tools of ~~cardiology~~ ^{medicine} in spite of being
limited to recording from pts. ^{or} completely, still ~~is~~

relaxed as possible and for only a short period
~~because of~~ | This was dictated by
of time, Technical limitations of recorders. There

have been many efforts. ~~These limitations have~~
~~✗~~ ^{Maurer's test}
long been recognized. By means of simple radio

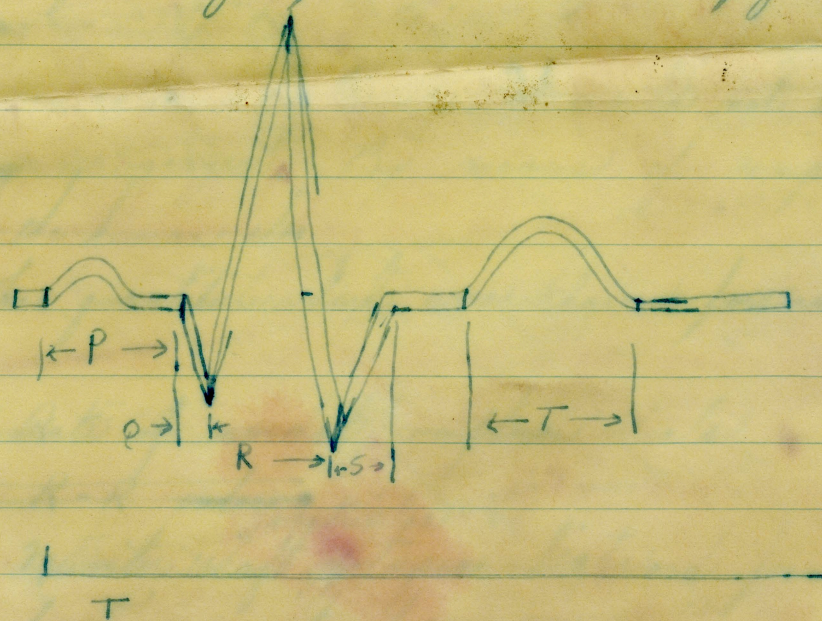
telemetry and magnetic tape recording we are now
able to obtain EKG records from individuals undergoing
almost any activity short of swimming and for periods
of many days. This has proven to be of great value
in both clinical practice and research.

The nature of the EKG requires ^{beginning}
~~even~~ It was evident from the ~~start~~ that
some methods of automatic data reduction would be
required. The typical record the typical record

previously occupied only a relatively few seconds
and whereas we were often faced with single records lasting
12 hrs. or more.

It may be worth the effort at this
point to briefly describe some pertinent aspects of
the EKG signal. The signal shown here
is from the telemetry or 'T' lead used by us. (illus.?)

The signal will vary of course with lead configuration
and



Appendix

The P wave represents the potential over associated
originates in the S.A. node,
the wave of biochemical activity which sweeps over the
atria of the heart and causes the muscular contraction
a few fraction of a second later. After a delay

There have been a number of publications on the analysis automatic analysis of the EKG but they usually were methods of data translation and programming such that the analysis could be performed by large conventional digital units or else they were in terms not familiar or accepted by the profession. It was desired to have a unit which was inexpensive, ^{small &} simple and would quantitate the desired features of the EKG in conventional terms. It would not attempt to supplant the human observer.

The quantities which were chosen for analysis were

1. Rate of normal complexes
2. R-R ~~intervals~~ ^{ventricular}
2. Number of ectopic beats
3. S-T segment depression
4. R-R intervals

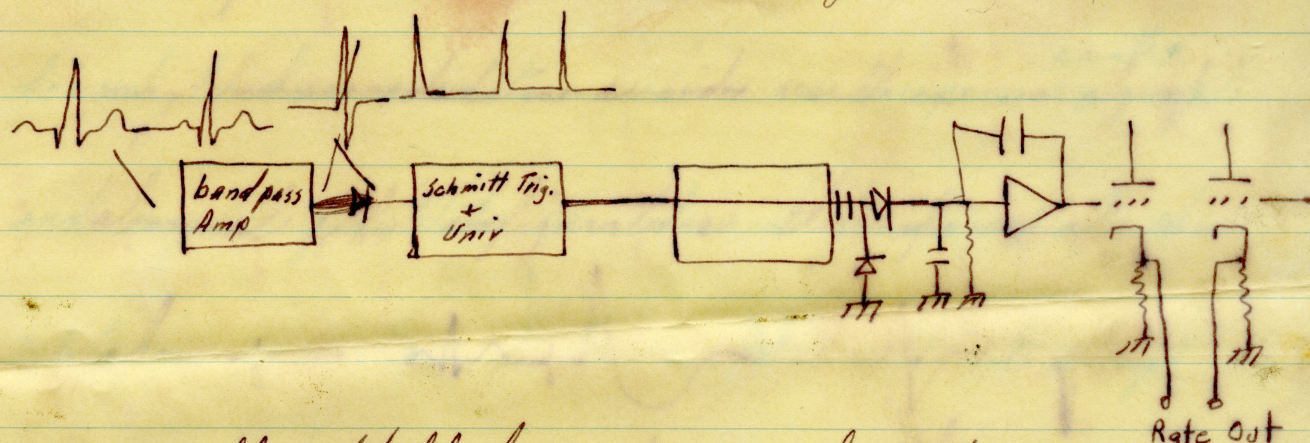
During normal activity

Rate: The portion QRS complex, particularly the 'R' wave provides the most reliable information pt. of and is the most constant feature of the record the record's ~~I in normal~~ ~~It is~~ ~~I in normal activity~~ as from individual to individual especially in disease.

~~especially involving long runs of activity, as~~

Rate is ^{normally} ~~usually~~ taken as the number of beats for a given period of time, usually not less than 15 sec. ~~and~~ ^{expressed in terms of bts/min.}

The same thing was done here to the ^{normal} Q.R.S. complexes being counted and averaged over a 30 sec. epoch and expressed as bts/min in analog voltage -

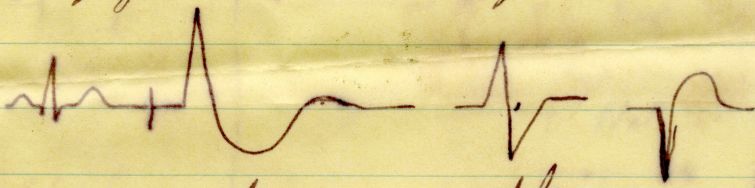


An abbreviated block diagram of the portion is shown and consists of a more or less conventional rate meter & a pulse average circuit. After careful empirical adjustment (i.e. a great deal of deck box after less than dozen

By proper selection of bandpass freq. - and the meter would count reliably in face of interference that rendered ^{visual} made recognition of the QRS complexes difficult.

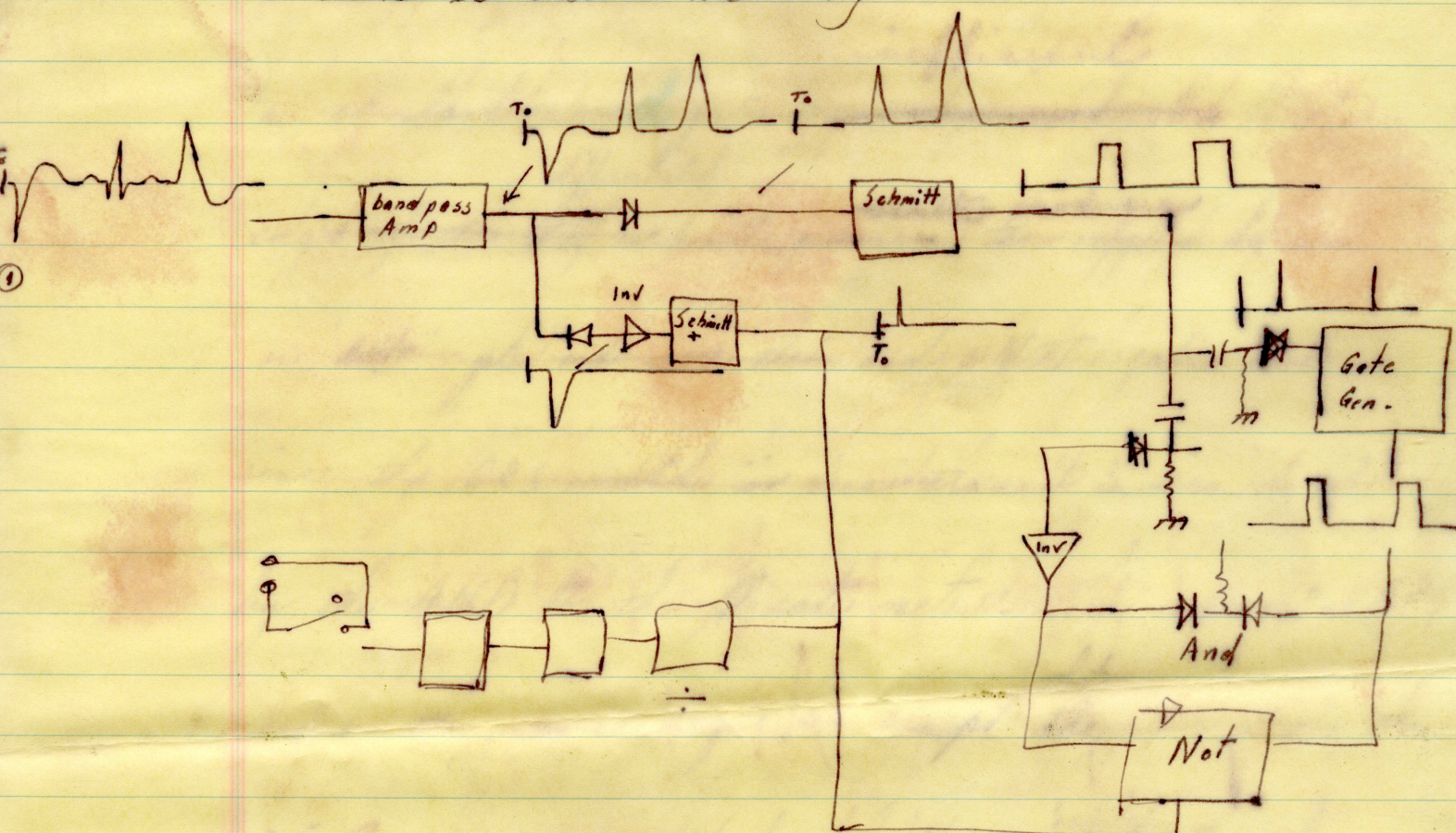
2. Ventricular Ectopic beats - These are ~~aberrant~~

abnormal contractions arising from a hypersensitive
area somewhere
near focus in the ventricles which produce a
trigger foci of excitation which spreads over
the heart causing an ^{inefficient} ~~poorly~~ coordinated beats.
Since these foci this ~~causes~~ ^{results produces} an entirely different
~~and~~ unpredictable for vector loops which ~~is~~ ^{is} ~~recor~~
may be recorded in a wide result in variety of

abnormal QRS configurations three of which are
shown - 

A common ~~feature~~ ^{useful} feature here
is a widened QRS interval. ~~It was~~ This feature
was chosen ~~so~~ to discriminate between these and normal
complexes. Another difficulty however was that ^{ectopic} ~~this~~ complex
was ^{sometimes} negative going. However the lead configuration gave
^{normal}
or could be adjusted to give QRS complexes a relatively low
amplitude QRS negative going components. Two criteria
are used to count V.E.B.s, ① a QRS amplitude

complex wider than .05 sec. at half amplitude
 or 2. a negative going QRS complex - The
 block is shown in Fig -

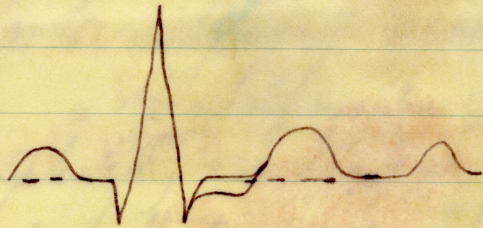


The three conditions which may exist are shown
 here - ① is a VEP & neg. going complex. This
 is passed ~~on to~~ by the diode ~~D2~~ but blocked by ~~D1~~.
 After passing ~~D2~~ it produces a single trigger and is
 counted by the binary chain. A normal complex is
 shown at ②. This is passed by ~~D1~~ and it
 produces a trigger for the constant width gate
 generator which produces triggers the schmitt which

produces a pulse equal to the $\frac{1}{2}$ amplitude width of the QRS complex. In addition the pulse & this pulse is differentiated and the leading edge triggers a constant width gate generator. The trailing edge of the ~~the~~^{differentiated} schmitt pulse is then applied to an 'AND' gate ~~and since the~~ and NOT gates and since the QRS width is less than .05 sec is passed by the 'AND' to the rate meter. The upright VEP's follow the same sequence except ~~that~~^{that} they are wider than .05 sec. & are passed by the 'NOT' gate to the VEP binaries - These binaries ^{have icons on the front panel} count up to 7 while the 8th pulse closes a relay to pass every 8th count to a recorder -

~~Most difficult~~
S.I. Segment depression - This was the most difficult of measurements to make. First there is some disagreement as to definition significance. A typical Although there is

If the segment between the Q + T segments
^{below the isoelectric line}
is depressed, it is an indication that the heart
(Infarction?)
is not receiving sufficient oxygen. The problem



then is to compare the amplitude of the ST segment to the
isoelectric line. Because ~~of~~ extremely small variations are
of importance and the base line may vary it is necessary
to do this on a beat to beat basis. At normal rates
the ~~ST~~ T-P and P-Q segments are both isoelectric but
at high rates $Q < T-P$ and the complexes merge so it was
necessary to use the P-Q segment - As previously stated the
only reliable timing point source is the QRS complex but
this followed the desired sample point (PQ). After studying
analysis of a large sample of EKG's showed
that the interval did not end less than .035 sec
before before the $\frac{1}{2}$ amplitude point of the positive going

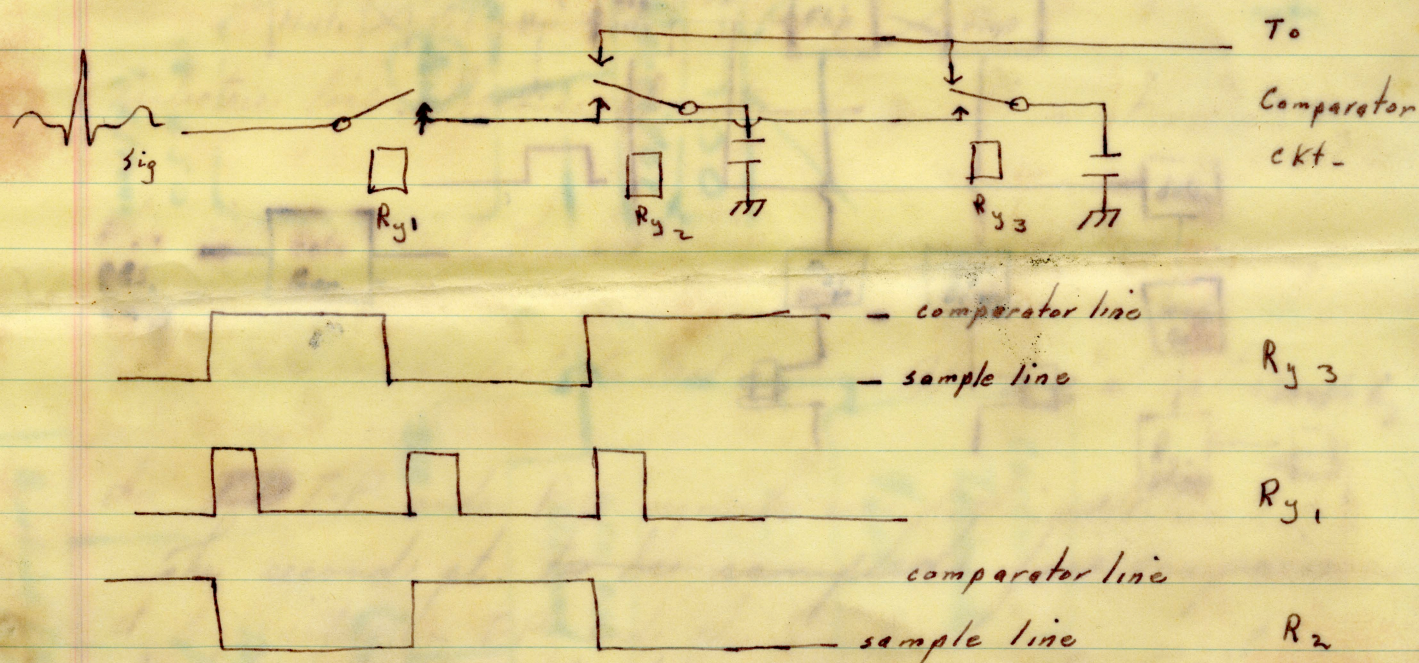
portion of the R nor did it begin less than .09 sec.
^{the segment is}
earlier. ~~no~~. Since ~~it was~~ flat a point chosen at

random between .04 and .08 sec. ahead of the (R)

~~would~~ ^{could} give a sample of the isoelectric amplitude.

^{memory capacitors $C_1 + C_2$}

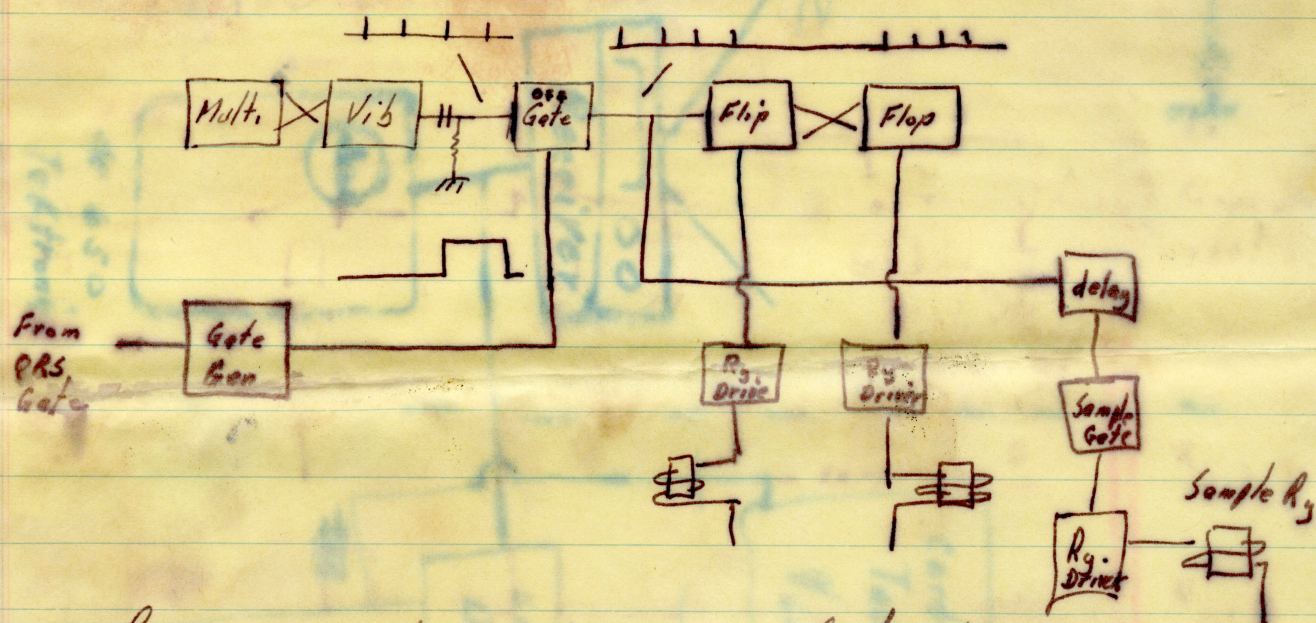
A sample R_y and two transfer relays were
in dwell times as shown.
arranged as shown in the



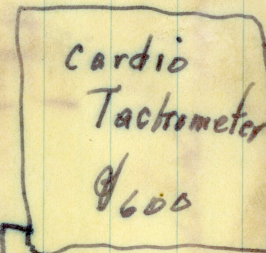
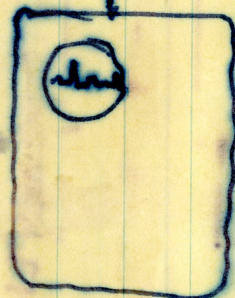
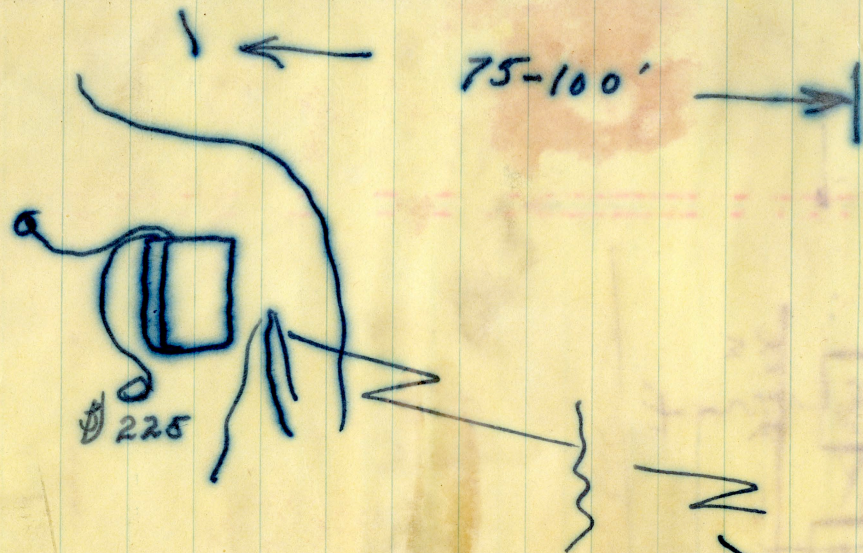
It can be seen that in this arrangement a sample cannot
be made available less than 35 msec after the sample point
nor be kept available more than 75 msec after this point.

The relays are held run at the rate shown sampling
at random in respect to the complexes. They are stopped
on by the R wave wave and held in this

this position is one of the other memory condensers available. This capacitor contains a sample made .035 to .075 sec. prior to the R wave or in other words a sample of the P-R interval which is isoelectric. ~~Two~~ Blocks for this are shown below -

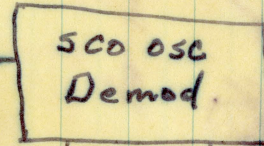


The second pt. to be sampled for comparison is the determined ~~determined~~ is the ~~junction~~ ^{reg.} point (j pt.) of the S to the T.

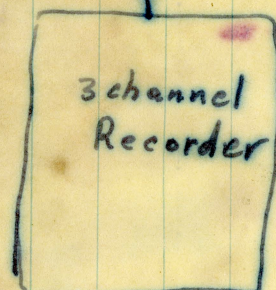
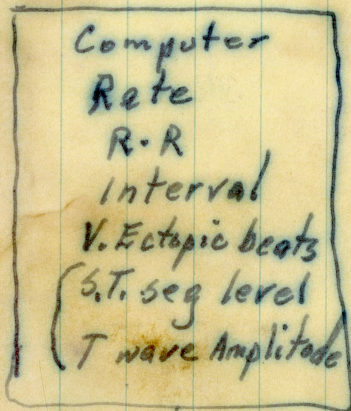
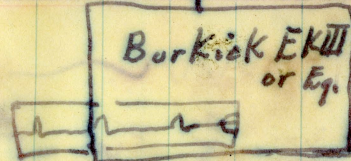


Rate

*325 to \$500



single
Track



\$2000

#1

#2

#3

